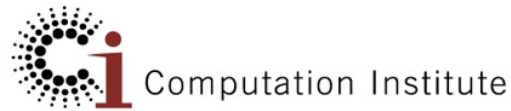


Sampling and Visualizing Creases with Scale-Space Particles

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FMRIB Centre
John Radcliffe Hospital
Oxford University
Stephen M. Smith

Outline

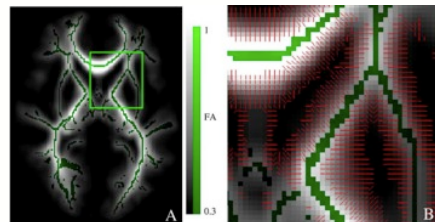
- **Introduction:** motivation, example, contributions
- **Method:** interpolation, features, energy, visualization, computation
- **Results:** lung CT, brain DTI, more
- **Discussion:** scale, particles, analysis, future

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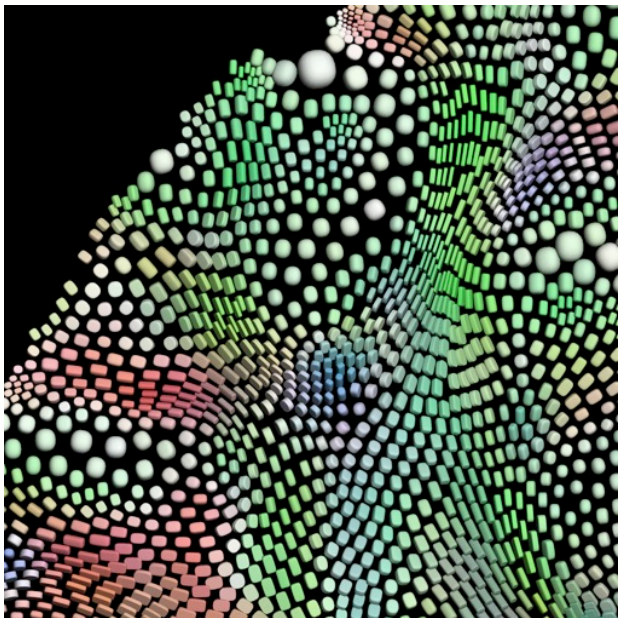
Context & Motivation

- Medical imaging is for measuring
- Often need “skeletons” of structures:
 - Ridges & valleys = creases
- Lung CT: find airways, measure radii, study COPD
- Brain DTI: find major WM tracts, measure FA, study psychiatric disorders
 - DTI not just for tractography
 - Much of it for FA studies
- Our initial work strives to be a general approach to detecting and sampling crease features

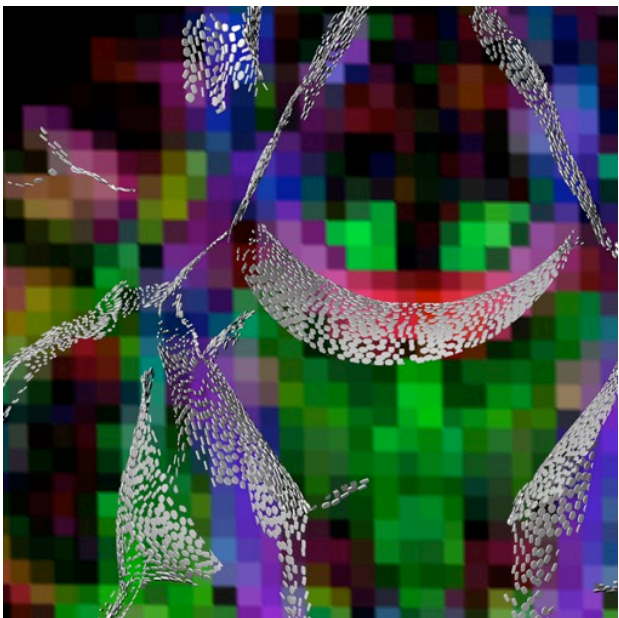


Take-aways

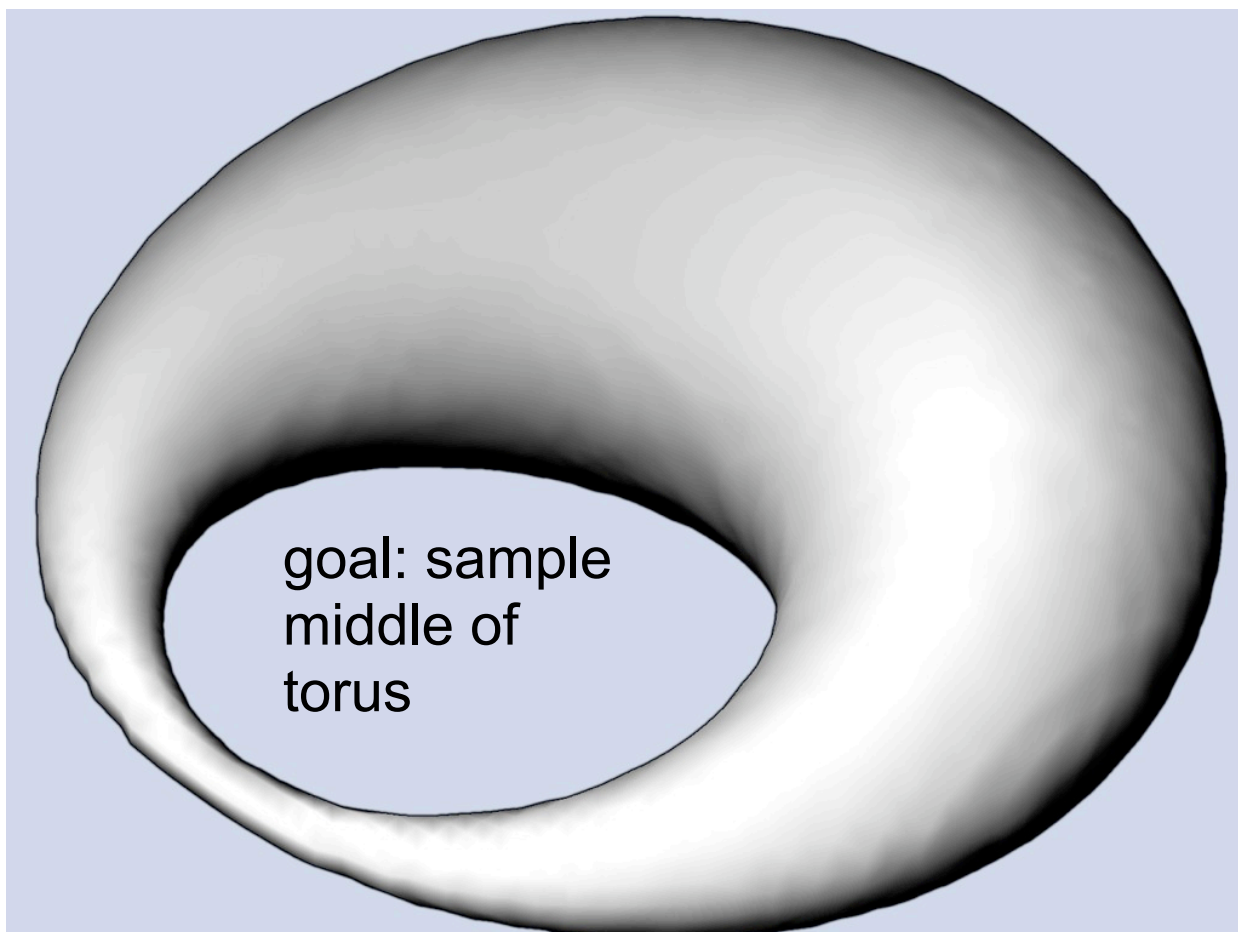
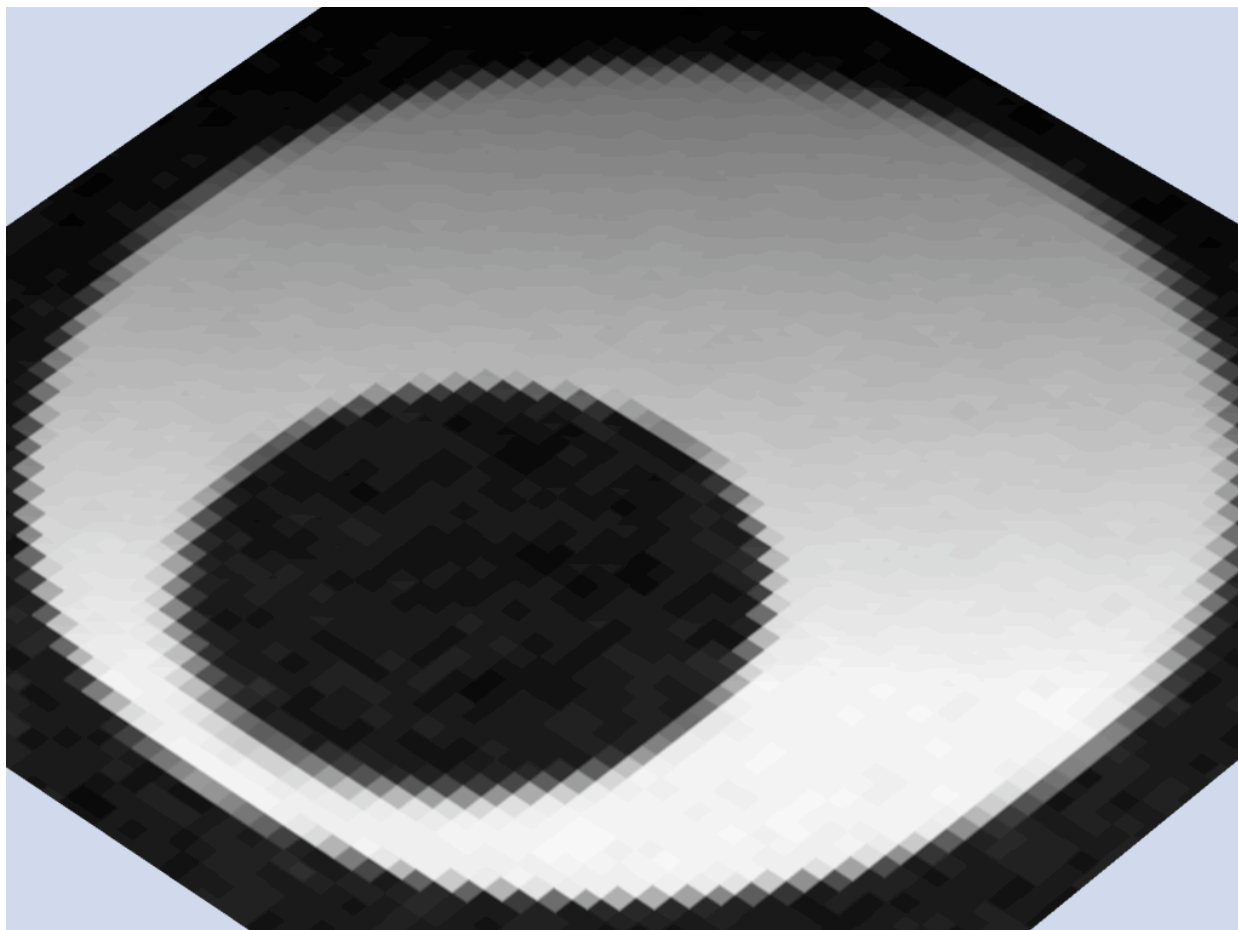
- Scale-space is useful, now more efficient in 3D
- Particles are natural for scale-space features
- Visualization as tool for design of image analysis

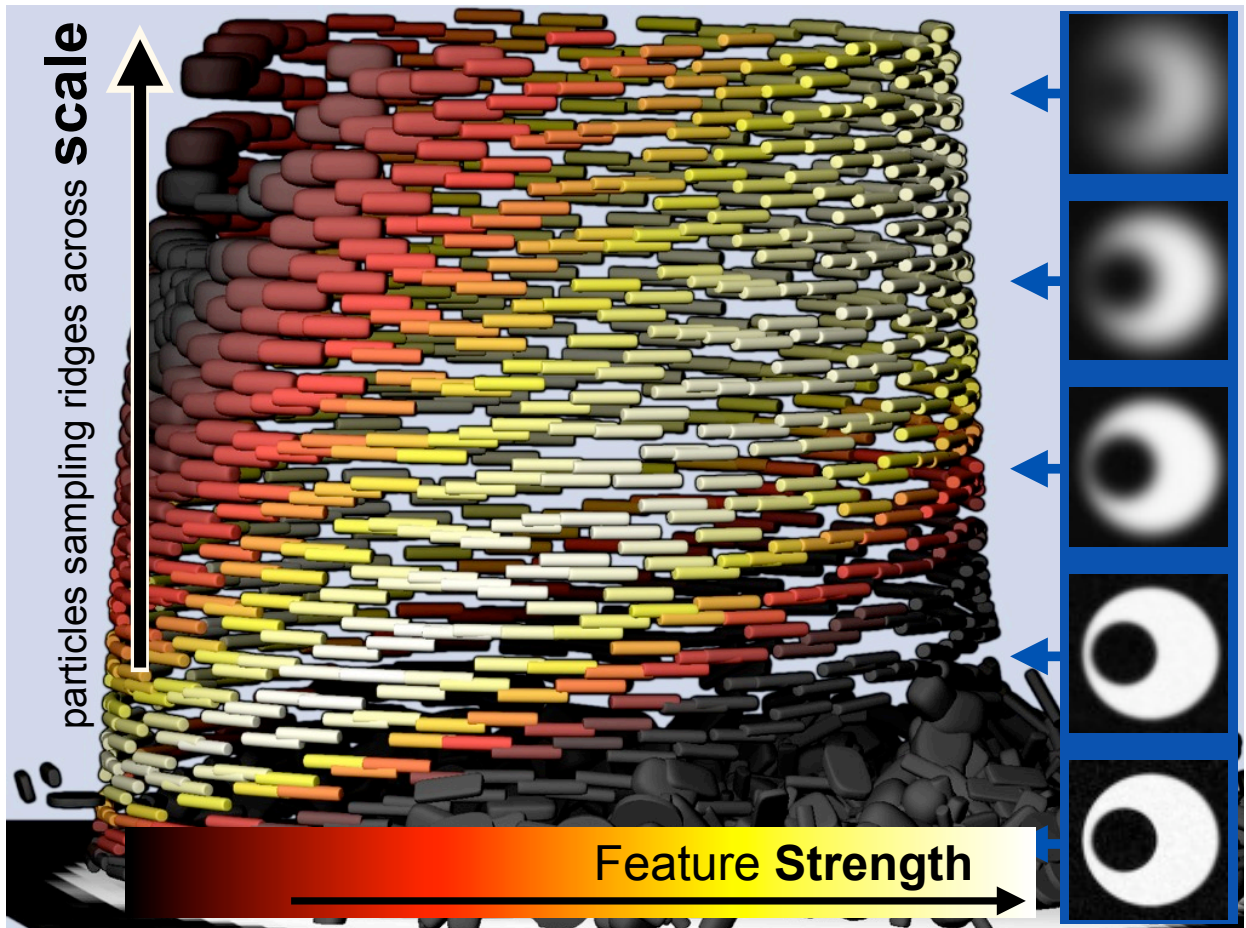
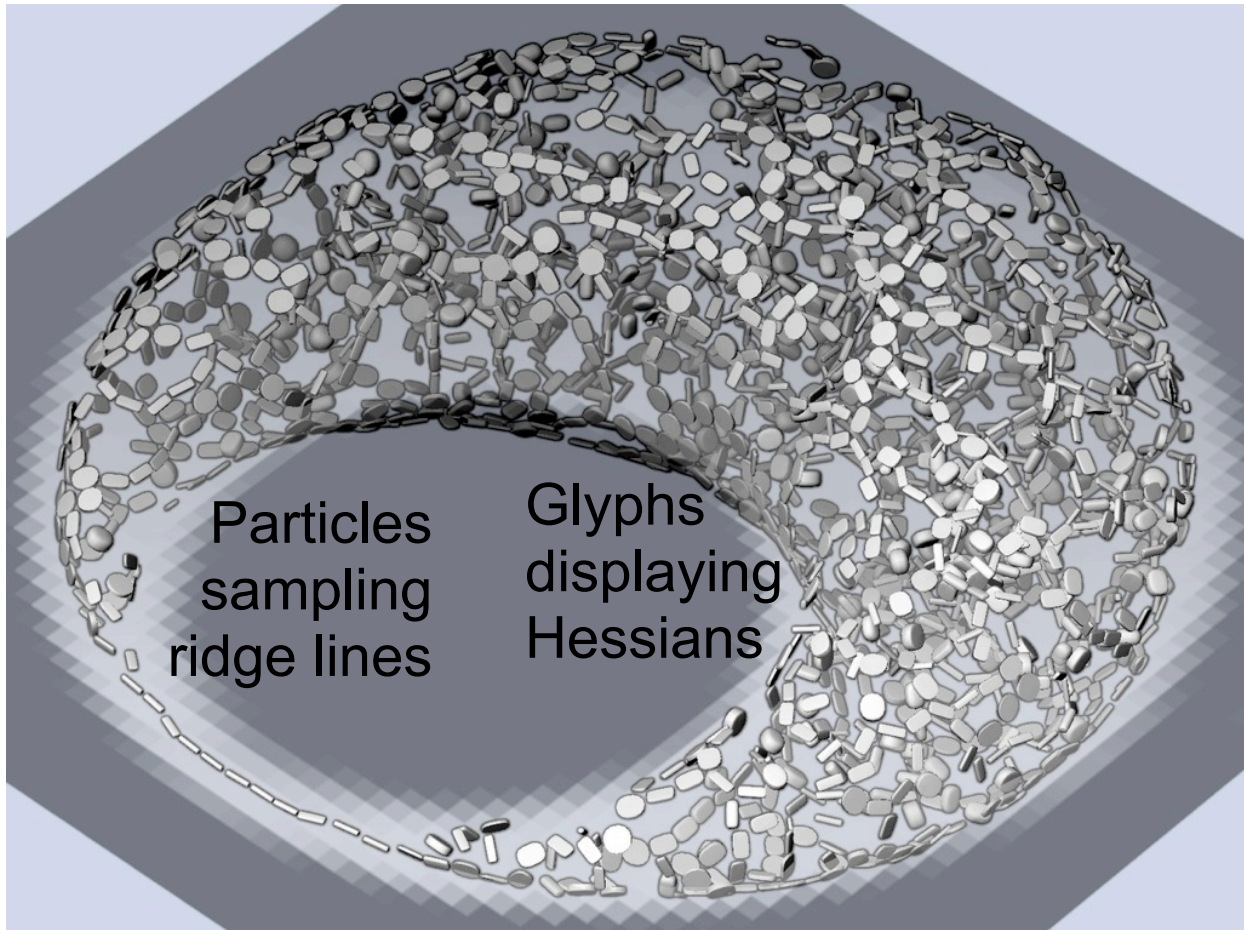


Particles for DTI visualization
(previous work, "Glyph Packing" Vis '06)
Glyphs for diffusion tensors
Sampling whole field
Image for humans to look at

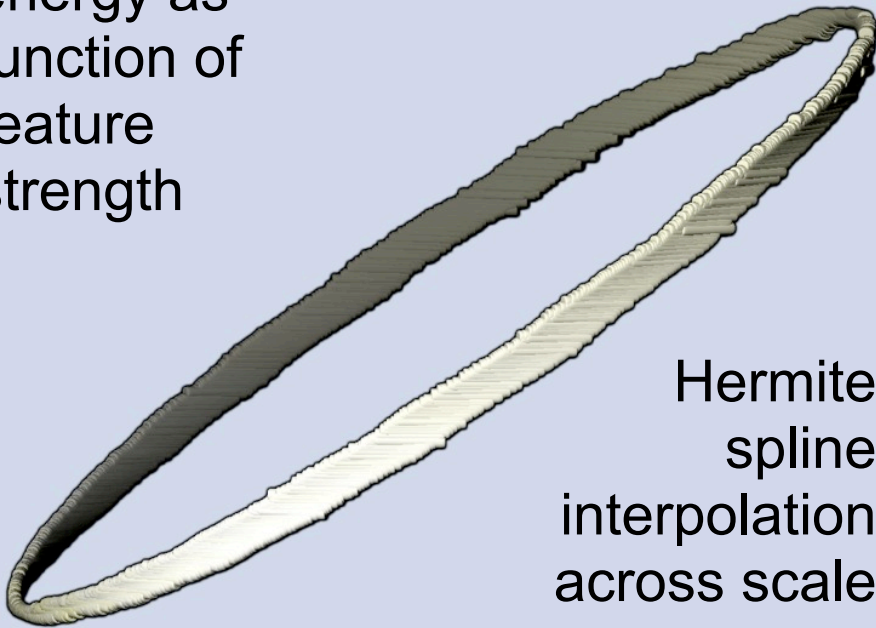


Particles for DTI analysis
(current work)
Glyphs for Hessians of FA
Sampling crease features
Geometry for measurement

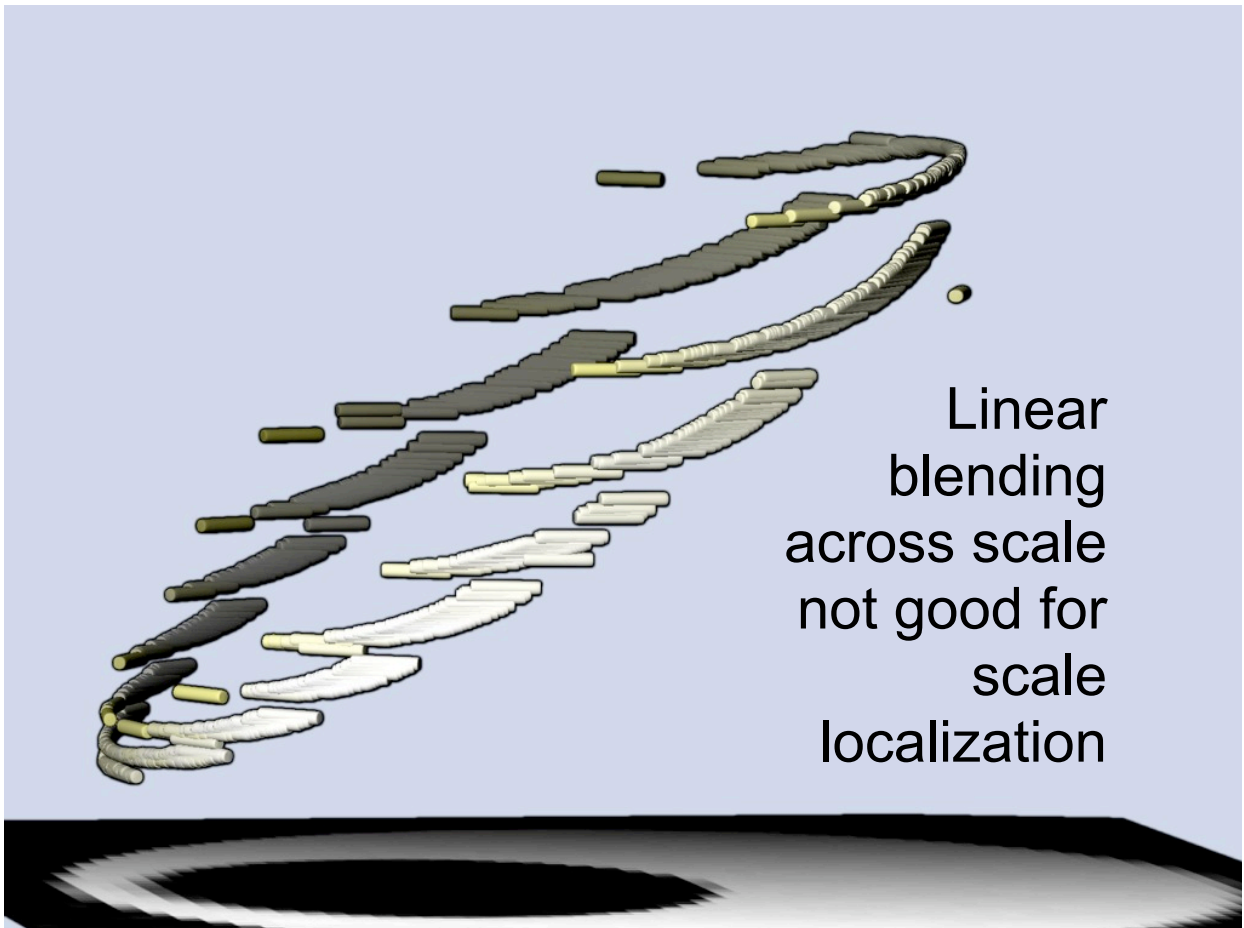
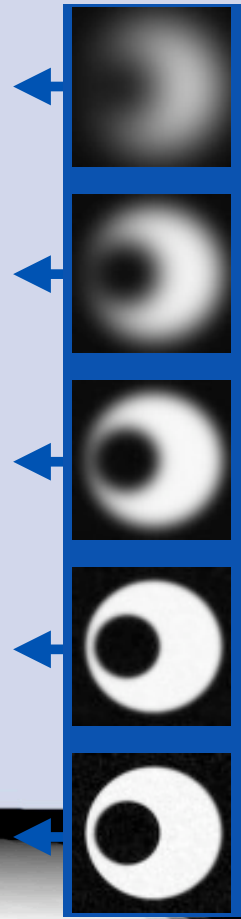




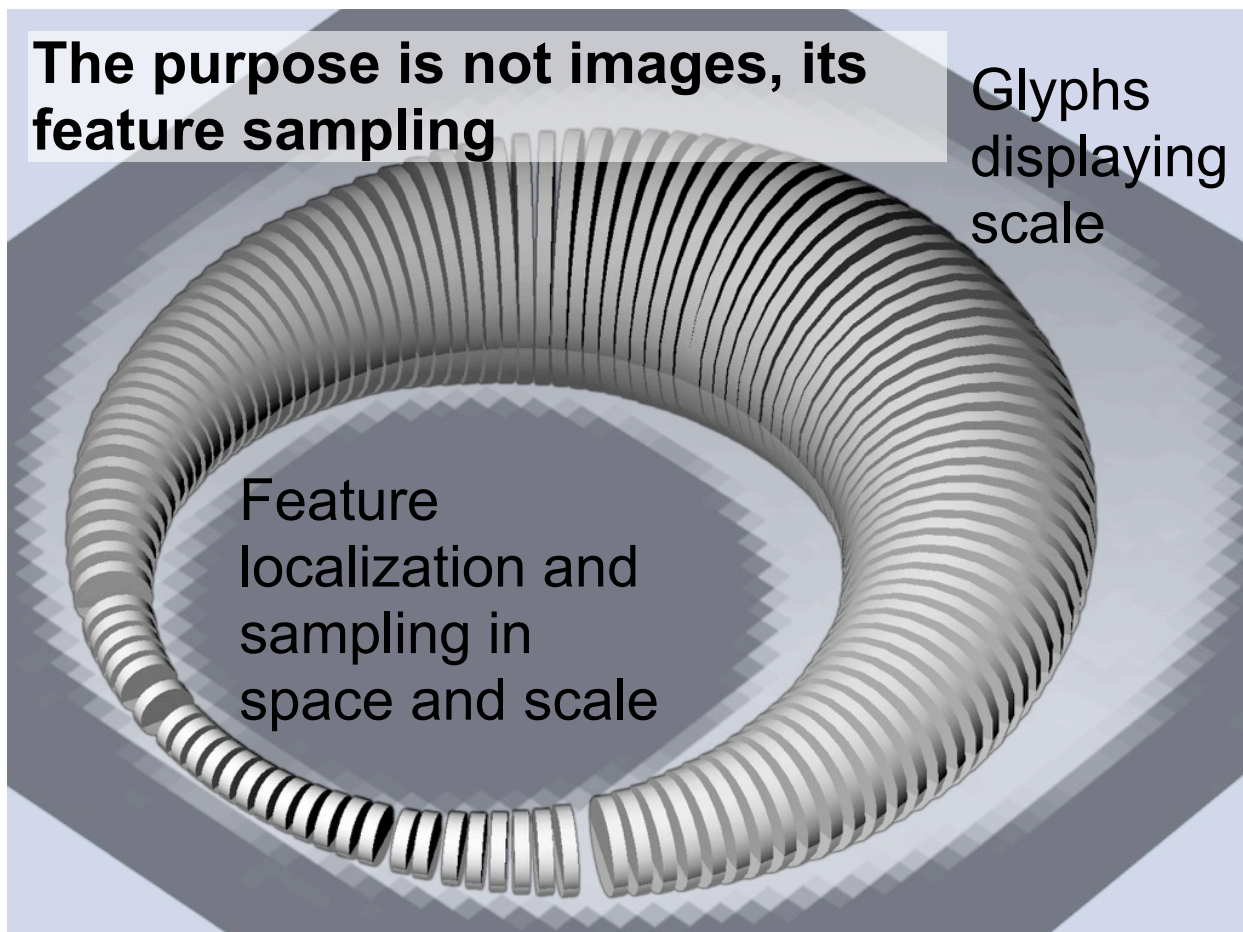
Particle-Image
energy as
function of
feature
strength



Hermite
spline
interpolation
across scale



Linear
blending
across scale
not good for
scale
localization



Contributions

- Efficient interpolation of scale for 3D images
- Particle-based sampling of ridges and valleys, in scale-space (vs. implicit surfaces, at single scale)
 - Energies that implement scale-localization
- Glyphs for depicting Hessians and/or scale
- Scale-space feature extraction in DTI

Not doing

- Meshing
 - Particles separate locations from connectivity
 - Meyer, Whitaker et al. 2005-2008
- Detailed comparison to application-specific segmentation methods
 - More general features, in various domains
- Performance optimization
 - Reference implementation, needs GPUs

Outline

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Method Overview

- Governing equation
- Interpolation: discrete to continuous, scale & space
- Crease feature constraints and strengths
- Particle-Image energy
- Inter-particle energy
- System visualization and dynamics

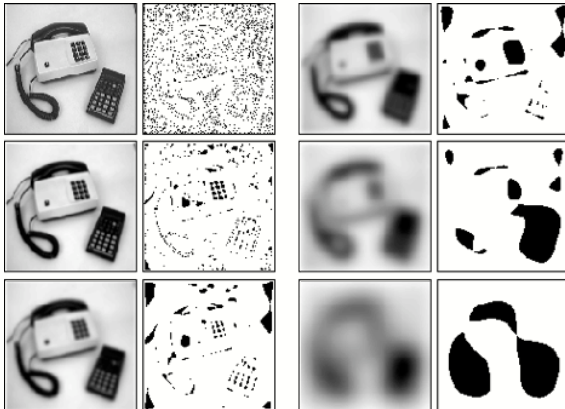
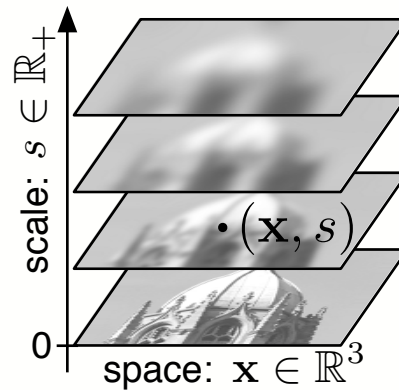
Governing equation

$$\underset{\underbrace{\{(\mathbf{x}_i, s_i)\}, N}_{\text{Particle positions}}}{\text{argmin}} \mathcal{E} = \underset{\underbrace{\{(\mathbf{x}_i, s_i)\}, N}_{\text{Particle number}}}{\text{argmin}} (1 - \alpha) \underbrace{\sum_{i=1}^N E_i}_{\text{Particle-image energy: localizes feature scale}} + \frac{\alpha}{2} \underbrace{\sum_{i,j=1}^N E_{ij}}_{\text{Inter-particle energy: induces uniform spatial sampling}}$$

- Feature constraints: enforced without contributing to energy
- Population control (finding N) becomes side-effect of energy minimization

Scale-Space

- From '90s computer vision
- Image and all possible **blurrings**
- More general than multi-resolution methods: scale is **continuous**



Structures of different sizes are naturally extracted at different scales

Tony Lindeberg '96

Scale-Space And Diffusion

- Various considerations lead to blurring with a **Gaussian**
- Image $L(x)$ diffuses for time $t \rightarrow$ continuum of images $L(x;t)$

$$L(x;t) = (L(\cdot) \star g(\cdot;t))(x) = \int g(\xi;t)L(x - \xi)d\xi$$

$$g(\xi;t) = \exp(-\xi^2/2t)/\sqrt{2\pi t}$$

- Heat equation: 1st deriv. in time \rightarrow 2nd deriv. in space

$$\frac{\partial L(x;t)}{\partial t} \propto \frac{\partial^2 L(x;t)}{\partial x^2}$$

- What's the analog in the **discrete** (implementation) domain?

Lindeberg's Discrete Gaussian

- “Scale-Space for Discrete Signals” IEEE PAMI 1990
- Beautiful analog to continuous Gaussian

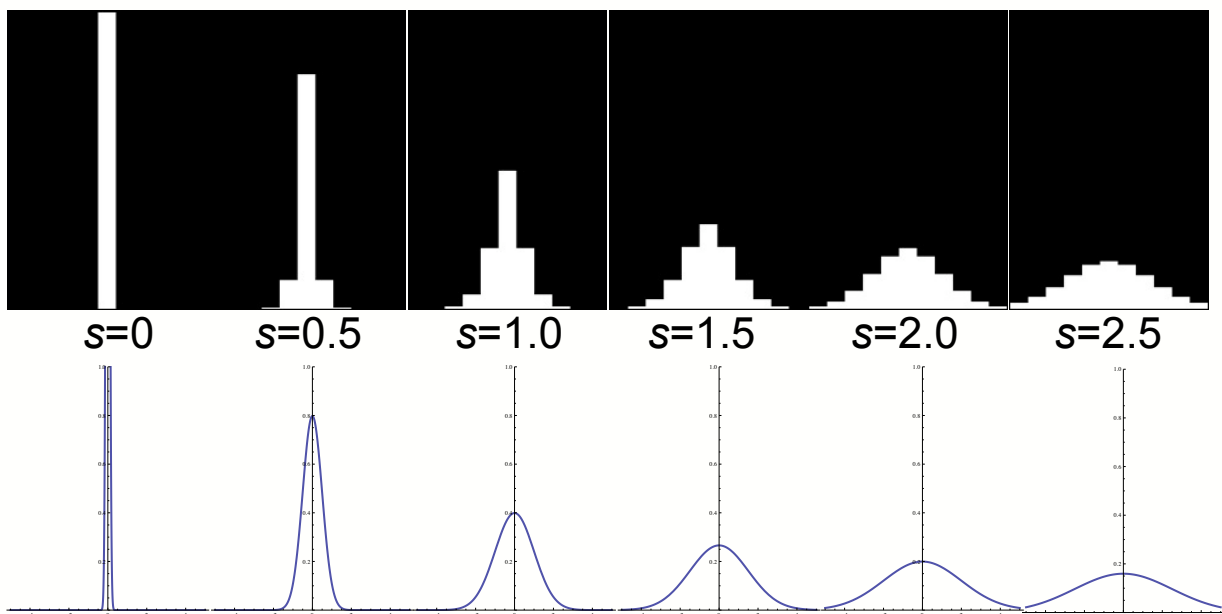
$$L[i; t] = (f \star K[\cdot; t])[i] = \sum_n K[n; t] f[i - n]$$

$$K[n; t] = \exp(-t) I_n(t); s = \sqrt{t} = \text{“}\sigma\text{”}$$

- $I_n(t)$ = modified Bessel function of order n

$$\begin{aligned} \frac{\partial K[i; t]}{\partial t} &= \frac{1}{2} (K[\cdot; t] \star [1 \quad -2 \quad 1])[i] \\ \Rightarrow \frac{\partial L[i; t]}{\partial t} &= \frac{1}{2} (L[\cdot; t] \star [1 \quad -2 \quad 1])[i] \\ \Rightarrow \frac{\partial L[i; s^2]}{\partial s} &= s (L[\cdot; s^2] \star [1 \quad -2 \quad 1])[i] \end{aligned}$$

Lindeberg's Discrete Gaussian



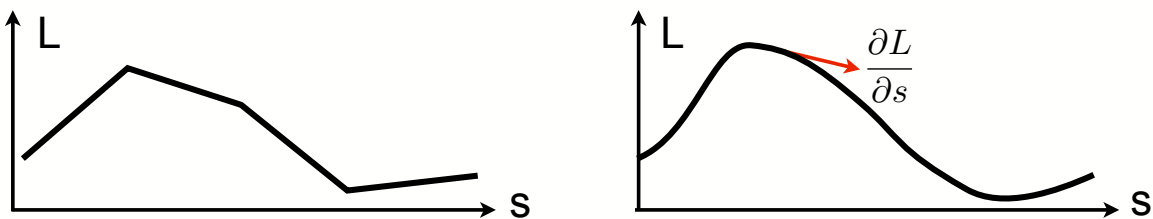
- Not the same as sampling a Gaussian
- Change **between** blurring levels important

Interpolate along scale

- We leverage properties of Lindeberg's Gaussian

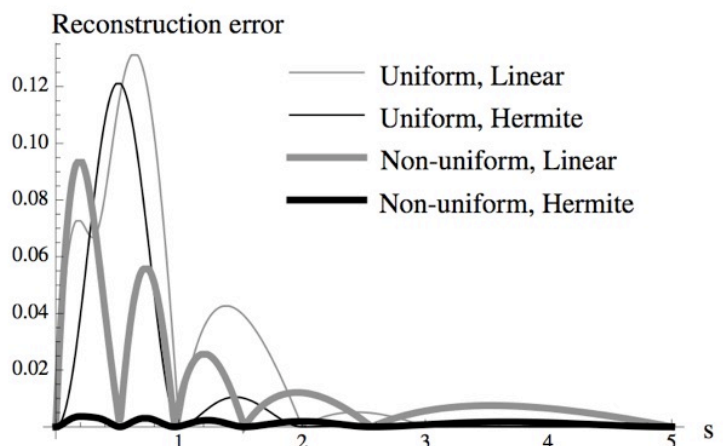
$$\frac{\partial L}{\partial s} = s (L[\cdot; s^2] \star [1 \quad -2 \quad 1])$$

- Pre-compute different blurrings of image L for discrete set of blurring levels
- For intermediate scales, could linearly blend between, or
- With dL/ds at each scale, create cubic **Hermite spline**



Scale interpolation accuracy

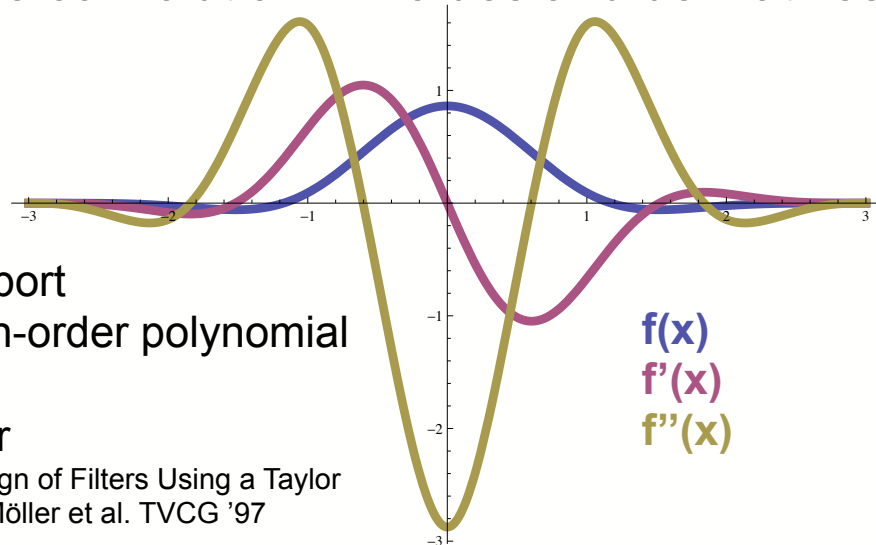
- Minimize number of pre-blurring volumes
- Measure error as squared difference between interpolated $K[]$ and true $K[]$, summed over support
- Optimize non-uniform scale sample locations by gradient descent on error



Hermite-spline scale interpolation makes scale-space practical for real-world 3D volumes

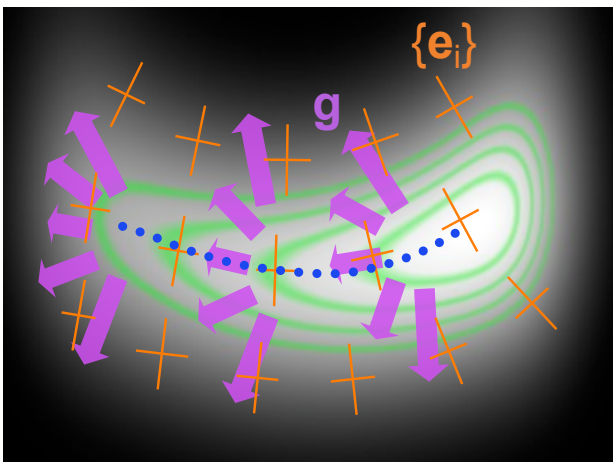
Spatial Interpolation

- At each particle location:
 - Scale interpolation → discrete spatial support
 - Separable convolution → values and derivatives



6-sample support
 Piece-wise 6th-order polynomial
 C^4 continuity
 4th-order error
 "Evaluation and Design of Filters Using a Taylor Series Expansion," Möller et al. TVCG '97

Ridges & Valleys = Creases



"Ridges in Image and Data Analysis" Eberly '96

Constrained extremum

Gradient \mathbf{g}

Hessian eigensystem \mathbf{e}_i, λ_i

Crease: \mathbf{g} orthogonal to one or more \mathbf{e}_i

Eigenvalue gives **strength**

Ridge surface: $\mathbf{g} \cdot \mathbf{e}_3 = 0$; $\lambda_3 < \text{thresh}$

Ridge line: $\mathbf{g} \cdot \mathbf{e}_3 = \mathbf{g} \cdot \mathbf{e}_2 = 0$; $\lambda_3, \lambda_2 < \text{thresh}$

Valley surface: $\mathbf{g} \cdot \mathbf{e}_1 = 0$; $\lambda_1 > \text{thresh}$

- Particles are **spatially** constrained to creases

Particle-Image Energy E_i

	RL	RS	VL	VS
Definition	$\mathbf{g} \cdot \mathbf{v}_2 = 0$ $\mathbf{g} \cdot \mathbf{v}_3 = 0$	$\mathbf{g} \cdot \mathbf{v}_3 = 0$	$\mathbf{g} \cdot \mathbf{v}_1 = 0$ $\mathbf{g} \cdot \mathbf{v}_2 = 0$	$\mathbf{g} \cdot \mathbf{v}_1 = 0$
λ sign	$\lambda_3 \leq \lambda_2 < 0$	$\lambda_3 < 0$	$0 < \lambda_2 \leq \lambda_1$	$0 < \lambda_1$
Strength h	$-\tilde{\lambda}_2$	$-\tilde{\lambda}_3$	$\tilde{\lambda}_2$	$\tilde{\lambda}_1$
Tangent \mathbf{T}	$\mathbf{v}_1 \otimes \mathbf{v}_1$	$\mathbf{v}_1 \otimes \mathbf{v}_1$ $+\mathbf{v}_2 \otimes \mathbf{v}_2$	$\mathbf{v}_3 \otimes \mathbf{v}_3$	$\mathbf{v}_2 \otimes \mathbf{v}_2$ $+\mathbf{v}_3 \otimes \mathbf{v}_3$

Ridge (R) and valley (V) surfaces (S) and lines (L)

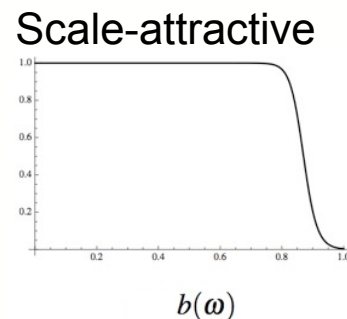
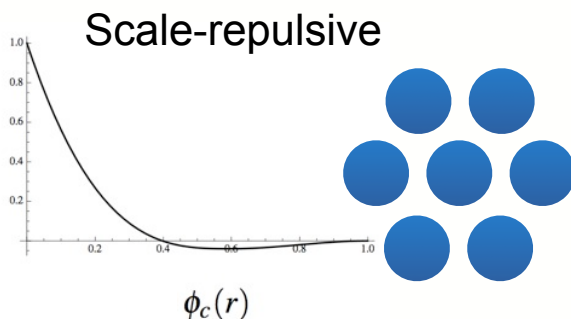
$$E_i = e(f, \mathbf{x}_i, s_i) = -\gamma h(\mathbf{x}_i, s_i)$$

- Particles migrate to maximal feature strength as part of energy minimization (not a constraint)

Inter-particle Energy E_{ij}

$$E_{ij} = \Phi(r_{ij}, s_{ij}) = \Phi\left(\frac{|\mathbf{x}_i - \mathbf{x}_j|}{\sigma_r}, \frac{s_i - s_j}{\sigma_s}\right)$$

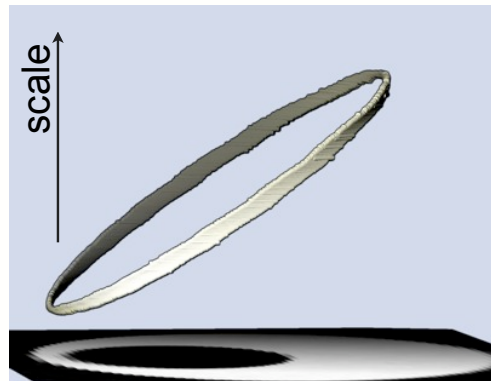
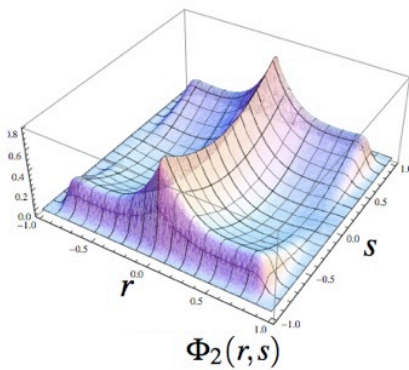
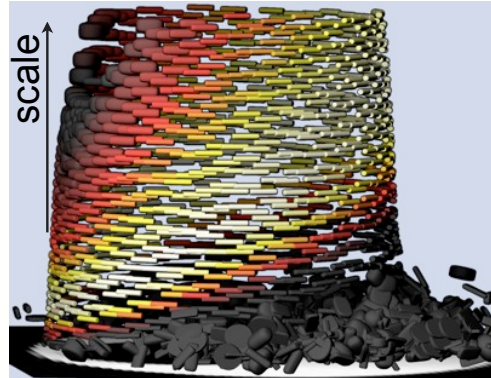
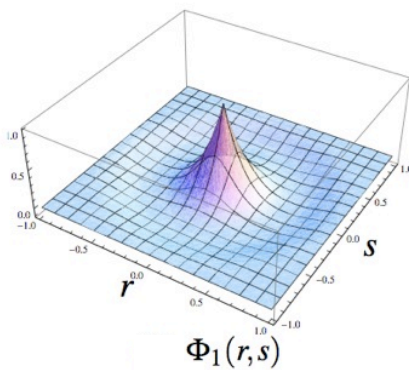
- No intrinsic orientation to particles' potential
- Have user-set "radii" in space σ_r and scale σ_s



$$\Phi_1(r, s) = \phi_c(\sqrt{r^2 + s^2})$$

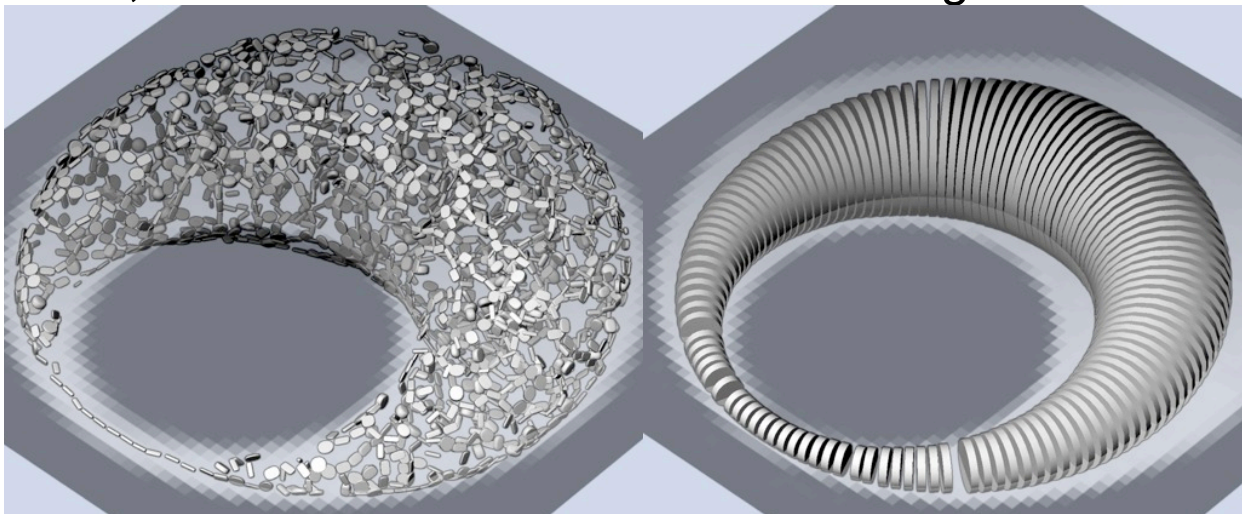
$$\Phi_2(r, s) = (1 - \beta)\phi_c(r)b(s) + \beta b(r)b(s)s^2$$

Inter-particle Energy E_{ij}



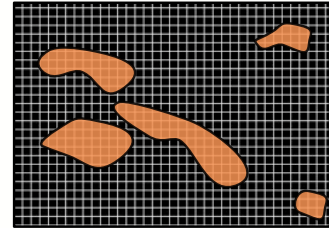
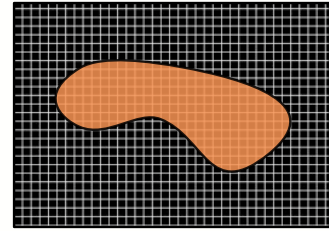
System Visualization

- Glyphs at particle locations, possibly colormapped
- Glyphs show tensors related to local Hessian
 - crease surfaces \rightarrow discs, lines \rightarrow rods
- Or, encode scale instead of Hessian eigenvalues



System Computation

- Initialize with particle at every Nth voxel
 - “CPM: A Deformable Model for Shape Recovery and Segmentation Based on Charged Particles” Jalba et al. IEEE PAMI '04
- Sampling one vs. detecting all
- Currently bottleneck
- Every iteration decreases energy
 - Move particles, with spatial constraint
 - Periodically try adding or nixing particles
- “Connected components”
 - Connected if non-zero inter-particle energy

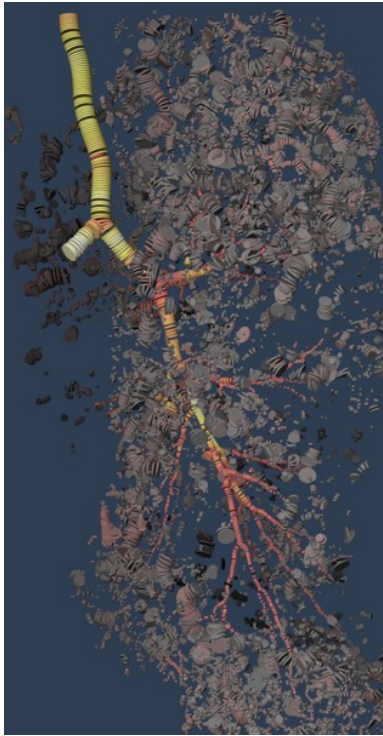


Outline

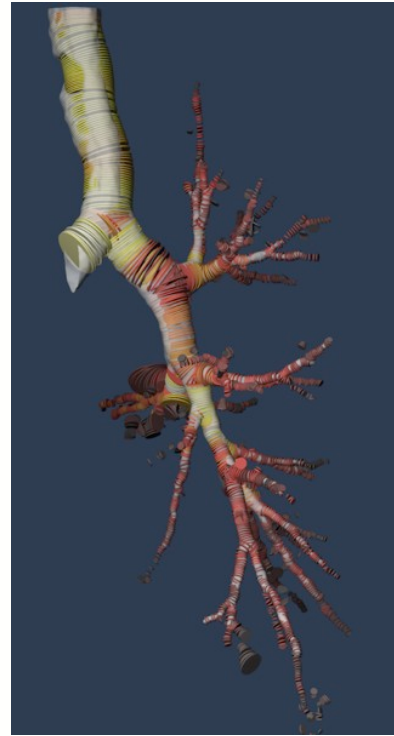
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Lung CT Results

- Lung airway segmentation still not quite solved
- Particles captured 4-5 levels of branching, as well as size



All CCs



Biggest CC

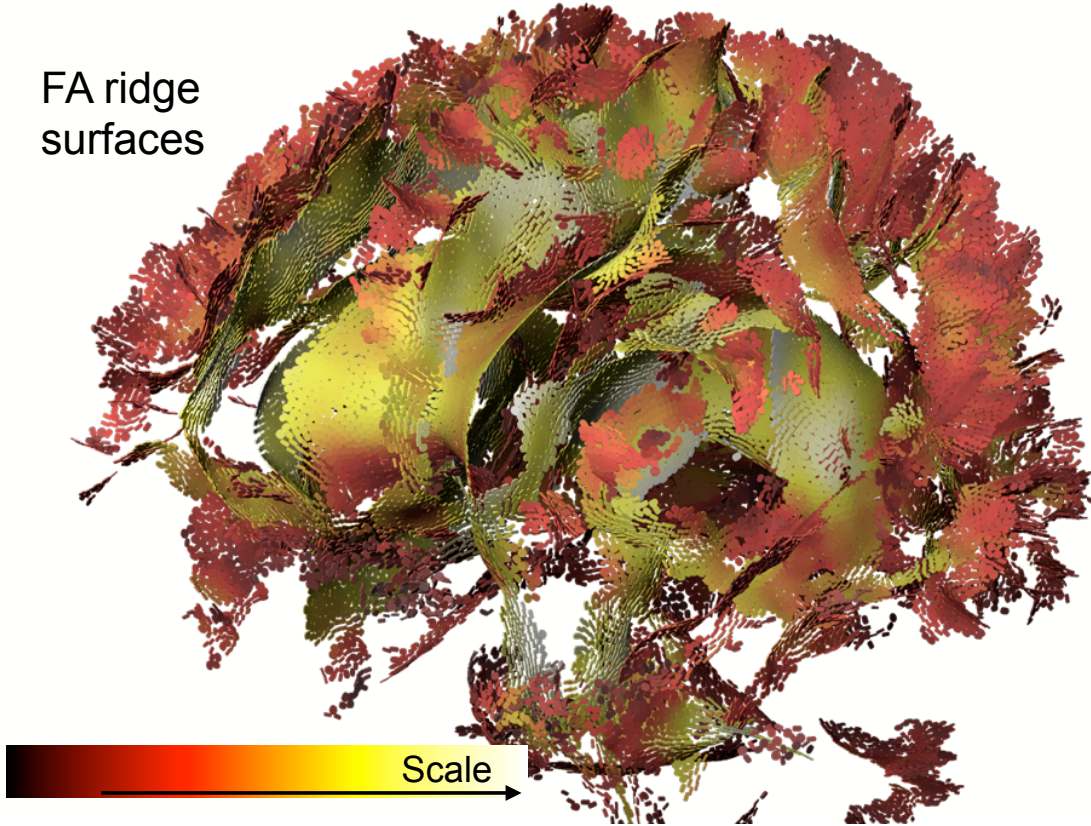
Lung CT Results



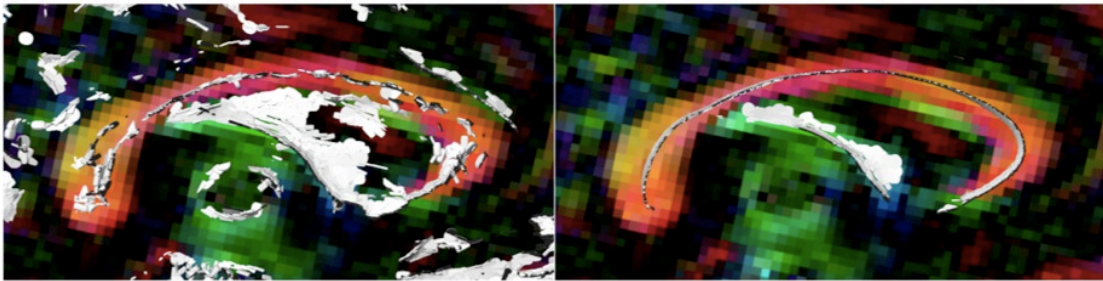
Smallest airways not much larger than voxels

Brain DTI Results

FA ridge surfaces



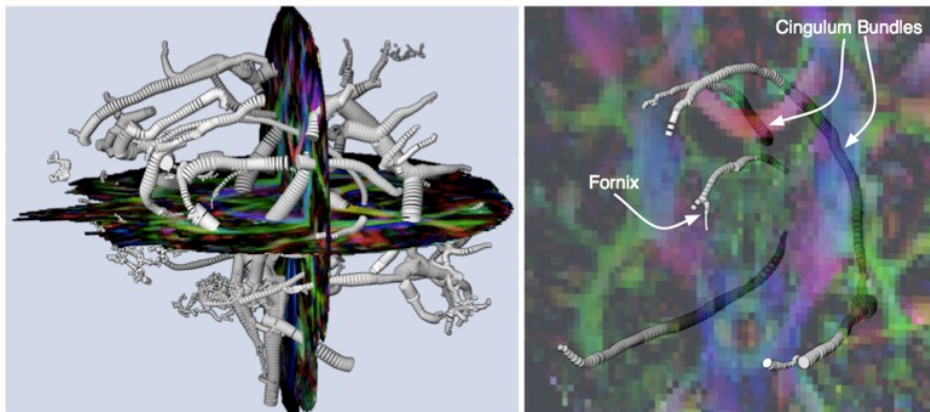
Brain DTI Results



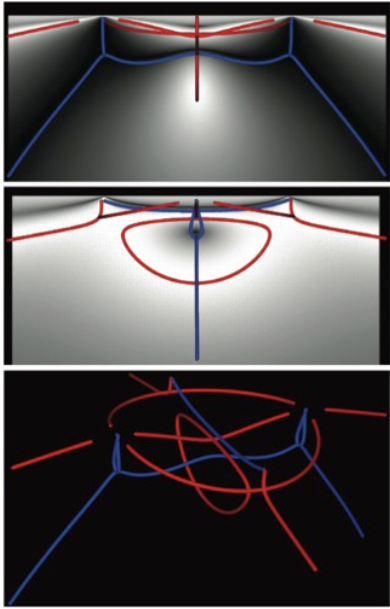
Without Scale-Space

With Scale-Space

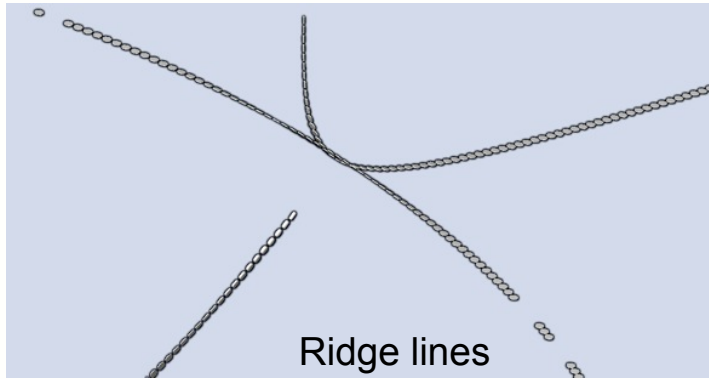
FA ridge lines



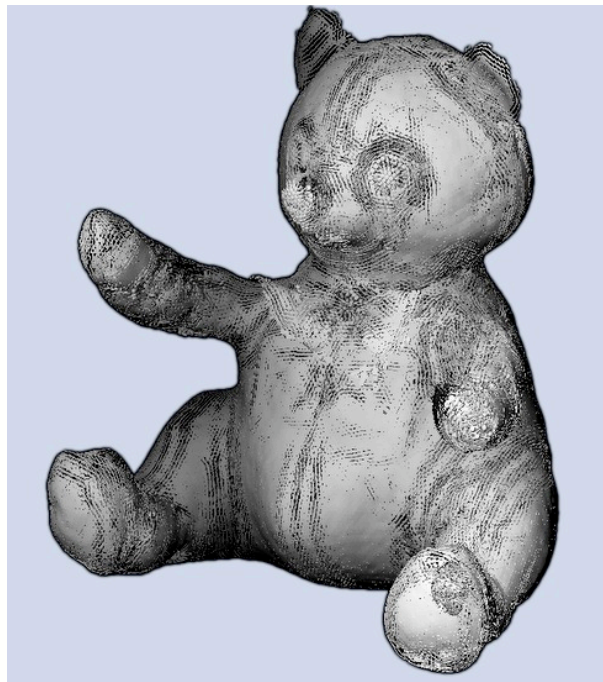
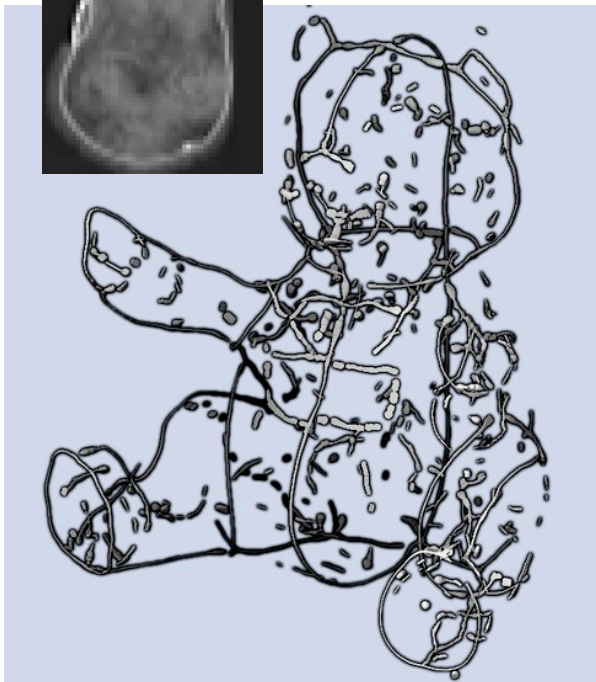
Double Point Load



“Invariant Crease Lines for Topological and Structural Analysis of Tensor Fields”
Tricoche et al. Vis '08



Teddy Bear

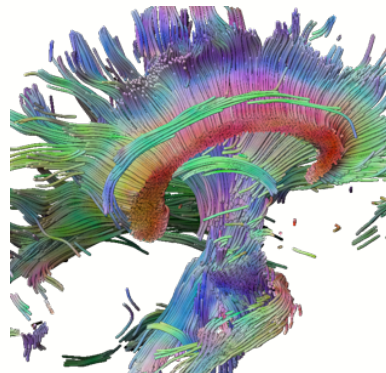
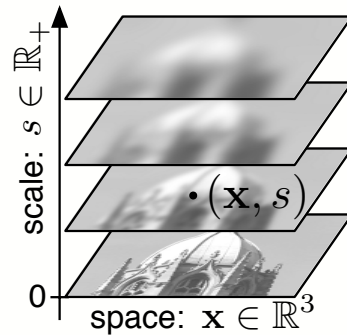


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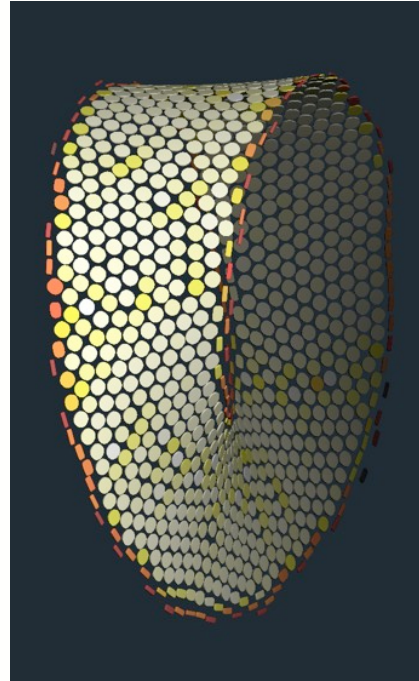
More Scale Space in Vis?

- Used some in visualization
 - “Surface Descriptors” session yesterday
 - Some feature tracking in flow fields
- Can always ask: but at what scale, and how stable WRT scale?



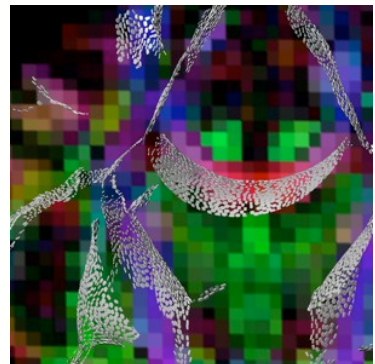
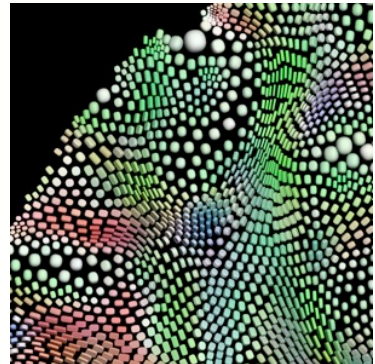
Joy of Particles

- Map from crease definition to particle motion
- Implement at level of individual particle behavior, watch group evolve
- Same system for curves or surfaces, with or without scale space



Visualization or Analysis?

- Intersection of both
- Vis, by **methods** (particles, glyphs) and **modality** (CT, DT-MRI)
- Vis & Analysis, by **strategy**: inspecting computation, feature detection, optimizing sampling
- Analysis, by **goals**: quantitative studies of local properties, shape variation, registration



Future work

- Other kinds of features: Canny edges
- Varying sampling density (curvature, local size)
- More parameter automation (did scale)
- Meshing, where needed
- GPU-based optimization

Acknowledgements

- Lung CT courtesy of Dr. George Washko, Brigham And Women's Hospital, Harvard Medical School
- Brain DTI courtesy of Dr. Kyle Pattinson, FMRIB Centre, Oxford University
- Funded by NIH grants U41-RR019703, U01-HL089856-02, P41-RR13218, and R01-MH074794.
- **Thank you for your attention**
- **Seeking grad student and post-doc**
- **Questions?**